Tracking Control for Neuromuscular Electrical Stimulation

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Problem and Our Solution

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Our new control only needs sampled observations, allows any delay, and tracks position and velocity under a state constraint.

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 $Y_t(\theta) = Y(t + \theta)$. Specify *u* to get a singly parameterized family $Y'(t) = \mathcal{G}(t, Y_t, \delta(t)), \quad Y(t) \in \mathcal{Y},$ (2) where $\mathcal{G}(t, Y_t, d) = \mathcal{F}(t, Y(t), u(t, Y(t - \tau)), d).$

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where $\mathcal{G}(t, Y_t, d) = \mathcal{F}(t, Y(t), u(t, Y(t - \tau)), d)$.

Typically we construct u such that all trajectories of (2) for all possible choices of δ satisfy some control objective.

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Find γ_i 's by building certain LKFs for $Y'(t) = \mathcal{G}(t, Y_t, 0)$.

What is a Lyapunov-Krasovskii Functional (LKF)?

Karafyllis (NTUA), Krstic (UCSD), Malisoff (LSU), et al. Tracking Control for Neuromuscular Electrical Stimulation

What is a Lyapunov-Krasovskii Functional (LKF)?

Definition: We call V^{\sharp} an ISS-LKF for $Y'(t) = \mathcal{G}(t, Y_t, \delta(t))$ provided there exist functions $\gamma_i \in \mathcal{K}_{\infty}$ such that

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$$\gamma_1(|\phi(0)|) \leq V^{\sharp}(t,\phi) \leq \gamma_2(|\phi|_{[-\tau,0]})$$

for all $(t,\phi) \in [0,\infty) \times \mathcal{C}([-\tau,0],\mathbb{R}^n)$

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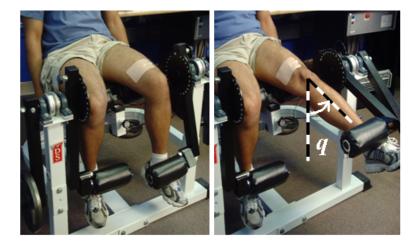
$$V^{\sharp}(Y_t) = V(Y(t)) + \frac{1}{4} \int_{t-\tau}^t |Y(\ell)|^2 \mathrm{d}\ell + \frac{1}{8\tau} \int_{t-\tau}^t \left[\int_s^t |Y(r)|^2 \mathrm{d}r \right] \mathrm{d}s$$

is an ISS-LKF for $Y'(t) = -Y(t) + \frac{1}{4}Y(t-\tau) + \delta(t)$.

(Loading Video...)

Leg extension machine at Warren Dixon's NCR Lab at U of FL

NMES on Leg Extension Machine



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 $M_e(q) = k_1 q e^{-k_2 q} + k_3 \tan(q)$: elastic effects due to joint stiffness with constants $k_i > 0$. We introduce the tan term to accommodate our state constraint $q \in (-\pi/2, \pi/2)$.

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 $M_g(q) = \mathcal{M}gl\sin(q)$: gravitational component. $\mathcal{M} =$ mass of shank and foot, g = gravitational acceleration, l = distance between knee-joint and lumped center of mass of shank-foot.

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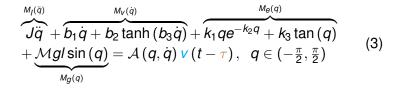
 $\mu = \zeta(q)F$: knee torque. F = total muscle force at tendon. $\zeta(q)$ = positive valued moment arm.

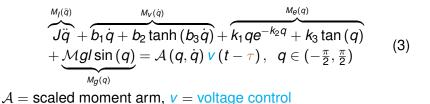
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 $F = \xi(q, \dot{q})v(t - \tau)$: v = voltage across quadriceps. τ = latency between applying voltage and force production.





$$\underbrace{J\ddot{q}}_{M_{g}(\ddot{q})} + \underbrace{b_{1}\dot{q} + b_{2} \tanh(b_{3}\dot{q})}_{M_{g}(q)} + \underbrace{k_{1}qe^{-k_{2}q} + k_{3}\tan(q)}_{M_{g}(q)} + \underbrace{\mathcal{M}gl\sin(q)}_{M_{g}(q)} = \mathcal{A}(q,\dot{q}) \vee (t-\tau), \quad q \in (-\frac{\pi}{2}, \frac{\pi}{2})$$
(3)

A = scaled moment arm, v = voltage control

$$\ddot{q}(t) = -\frac{dF}{dq}(q(t)) - H(\dot{q}(t)) + G(q(t), \dot{q}(t))v(t-\tau)$$
(4)

$$\underbrace{\overset{M_{l}(\ddot{q})}{J\ddot{q}} + \overset{M_{v}(\dot{q})}{b_{1}\dot{q} + b_{2}} \tanh(b_{3}\dot{q})}_{M_{g}(q)} + \underbrace{\mathcal{M}g/\sin(q)}_{M_{g}(q)} = \mathcal{A}(q,\dot{q}) \mathbf{v}(t-\tau), \quad q \in (-\frac{\pi}{2}, \frac{\pi}{2})}$$
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Our Requirements:

■ F : $(-\pi/2, \pi/2) \rightarrow [0, \infty)$ is C^2 and $\lim_{q \rightarrow \pm \pi/2} F(q) = \infty$. ■ G : $(-\pi/2, \pi/2) \times \mathbb{R} \rightarrow (0, \infty)$ is C^1 and bounded. ■ H : $\mathbb{R} \rightarrow \mathbb{R}$ is C^1 and $\inf_{x \in \mathbb{R}} x H(x) \ge 0$.

$$\ddot{q}(t) = -\frac{dF}{dq}(q(t)) - H(\dot{q}(t)) + G(q(t), \dot{q}(t))\mathbf{v}(t-\tau)$$
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$$F(q) = \frac{k_1 \exp(-k_2 q)}{Jk_2^2} \left(\exp(k_2 q) - 1 - k_2 q \right) \\ + \frac{mgl}{J} \left(1 - \cos(q) \right) + \frac{k_3}{J} \ln\left(\frac{1}{\cos(q)}\right),$$

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We want $(q - q_d, \dot{q} - \dot{q}_d) \rightarrow 0$ in a UGAS exponential way.

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Three parts of the control scheme, assuming $t_0 = 0$:

A numerical prediction $\xi(T_i) = z_{N_i}$ of the error variables at time $T_i + \tau$ using $(q(T_i), \dot{q}(T_i)) \in (-\pi/2, \pi/2) \times \mathbb{R}$.

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Applying the predictor feedback v(t), i.e., the nominal control with the state variables replaced by their predicted values.

 $v(t) = \frac{g_2(\zeta_d(t+\tau))v_d(t) - g_1(\zeta_d(t+\tau) + \xi(t)) + g_1(\zeta_d(t+\tau)) - (1+\mu^2)\xi_1(t) - 2\mu\xi_2(t)}{g_2(\zeta_d(t+\tau) + \xi(t))}$

for all $t \in [T_i, T_{i+1})$ and each *i*

$$\begin{split} \mathbf{v}(t) &= \frac{g_2(\zeta_d(t+\tau))\mathbf{v}_d(t) - g_1(\zeta_d(t+\tau) + \xi(t)) + g_1(\zeta_d(t+\tau)) - (1+\mu^2)\xi_1(t) - 2\mu\xi_2(t))}{g_2(\zeta_d(t+\tau) + \xi(t))} \\ \text{for all } t \in [T_i, T_{i+1}) \text{ and each } i, \text{ where} \\ g_1(x) &= -(1+x_1^2)\frac{dF}{dq}(\tan^{-1}(x_1)) + \frac{2x_1x_2^2}{1+x_1^2} - (1+x_1^2)H\left(\frac{x_2}{1+x_1^2}\right), \\ g_2(x) &= (1+x_1^2)G\left(\tan^{-1}(x_1), \frac{x_2}{1+x_1^2}\right), \\ \zeta_d(t) &= (\zeta_{1,d}(t), \zeta_{2,d}(t)) = \left(\tan(q_d(t)), \frac{\dot{q}_d(t)}{\cos^2(q_d(t))}\right), \\ \xi_1(t) &= e^{-\mu(t-T_i)}\left\{\left(\xi_2(T_i) + \mu\xi_1(T_i)\right)\sin(t-T_i) \right. \\ &+ \xi_1(T_i)\cos(t-T_i)\right\}, \\ \xi_2(t) &= e^{-\mu(t-T_i)}\left\{-\left(\mu\xi_2(T_i) + (1+\mu^2)\xi_1(T_i)\right)\sin(t-T_i) \right. \\ &+ \xi_2(T_i)\cos(t-T_i)\right\}, \\ \text{and } \xi(T_i) &= z_{N_i}. \end{split}$$

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and $\xi(T_i) = z_{N_i}$. The time-varying Euler iterations $\{z_k\}$ at each time T_i use measurements $(q(T_i), \dot{q}(T_i))$.

Voltage Potential Controller (continued)

Euler iterations used for control:

$$z_{k+1} = \Omega(T_i + kh_i, h_i, z_k; \mathbf{v}) \text{ for } k = 0, ..., N_i - 1 \text{, where}$$

$$z_0 = \begin{pmatrix} \tan(q(T_i)) - \tan(q_d(T_i)) \\ \frac{\dot{q}(T_i)}{\cos^2(q(T_i))} - \frac{\dot{q}_d(T_i)}{\cos^2(q_d(T_i))} \end{pmatrix}, \quad h_i = \frac{\tau}{N_i} \text{,}$$

and $\Omega:[0,+\infty)^2\times \mathbb{R}^2 \to \mathbb{R}^2$ is defined by

$$\Omega(T, h, x; \mathbf{v}) = \begin{bmatrix} \Omega_1(T, h, x; \mathbf{v}) \\ \Omega_2(T, h, x; \mathbf{v}) \end{bmatrix}$$
(8)

and the formulas

$$\begin{aligned} \Omega_1(T,h,x;v) &= x_1 + hx_2 \text{ and} \\ \Omega_2(T,h,x;v) &= x_2 + \zeta_{2,d}(T) + \int_T^{T+h} g_1(\zeta_d(s) + x) \mathrm{d}s \\ &+ \int_T^{T+h} g_2(\zeta_d(s) + x) v(s-\tau) \mathrm{d}s - \zeta_{2,d}(T+h). \end{aligned}$$

For all positive constants τ and r, there exist a locally bounded function N, a constant $\omega \in (0, \mu/2)$ and a locally Lipschitz function C satisfying C(0) = 0 such that: For all sample times $\{T_i\}$ in $[0, \infty)$ such that $\sup_{i \ge 0} (T_{i+1} - T_i) \le r$ and each initial condition, the solution $(q(t), \dot{q}(t), \mathbf{v}(t))$ with

$$N_{i} = N\left(\left|\left(\tan(q(T_{i})), \frac{\dot{q}(T_{i})}{\cos^{2}(q(T_{i}))}\right) - \zeta_{d}(T_{i})\right| + \left||\mathbf{v} - \mathbf{v}_{d}||_{[T_{i} - \tau, T_{i}]}\right)\right)$$
(9)

satisfies

$$\begin{aligned} |q(t) - q_d(t)| + |\dot{q}(t) - \dot{q}_d(t)| + ||\mathbf{v} - \mathbf{v}_d||_{[t-\tau,t]} \\ &\leq e^{-\omega t} C \left(\frac{|q(0) - q_d(0)| + |\dot{q}(0) - \dot{q}_d(0)|}{\cos^2(q(0))} + ||\mathbf{v}_0 - \mathbf{v}_d||_{[-\tau,0]} \right) \end{aligned}$$

for all $t \ge 0$.

Our main lemma gives general conditions on systems of the form $\dot{x}(t) = f(t, x(t), u(t))$ that allow us to predict future states of the system, using an explicit Euler method with iterates

$$x_{i+1} = x_i + \int_{t_0+ih}^{t_0+(i+1)h} f(s, x_i, u(s)) ds, \ 0 \le i \le N-1,$$
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where $h = \frac{\tau}{N}$, $x_0 \in \mathbb{R}^n$, and $u : [t_0, t_0 + \tau) \to \mathbb{R}^m$ are given.

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The lemma builds functions A_i such that for any $\tau > 0$, $x_0 \in \mathbb{R}^n$, $t_0 \ge 0$, and measurable bounded function $u : [t_0, t_0 + \tau) \to \mathbb{R}^m$, the solution of $\dot{x}(t) = f(t, x(t), u(t)), x(t_0) = x_0$ satisfies

$$|x(t_0 + \tau) - x_N| \leq \frac{\tau A_1(|x_0| + ||u||)}{N} (e^{\tau A_2(|x_0| + ||u||)} - 1)$$
(11)

for all $N \ge \tau A_3 (|x_0| + ||u||)$.

$$J\ddot{q} + b_1\dot{q} + b_2\tanh(b_3\dot{q}) + k_1qe^{-k_2q} + k_3\tan(q) + \mathcal{M}gl\sin(q) = \mathcal{A}(q,\dot{q}) v(t-\tau), \quad q \in (-\frac{\pi}{2}, \frac{\pi}{2})$$
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$$\tau = 0.07s, \,\mathcal{A}(q,\dot{q}) = \bar{a}e^{-2q^{2}}\sin(q) + \bar{b}$$

$$J = 0.39 \,\mathrm{kg} \cdot \mathrm{m}^{2}/\mathrm{rad}, \, b_{1} = 0.6 \,\mathrm{kg} \cdot \mathrm{m}^{2}/(\mathrm{rad} \cdot \mathrm{s}), \, \bar{a} = 0.058, \\ b_{2} = 0.1 \,\mathrm{kg} \cdot \mathrm{m}^{2}/(\mathrm{rad} \cdot \mathrm{s}), \, b_{3} = 50 \,\mathrm{s/rad}, \, \bar{b} = 0.0284, \\ k_{1} = 7.9 \,\mathrm{kg} \cdot \mathrm{m}^{2}/(\mathrm{rad} \cdot \mathrm{s}^{2}), \, k_{2} = 1.681/\mathrm{rad}, \\ k_{3} = 1.17 \,\mathrm{kg} \cdot \mathrm{m}^{2}/(\mathrm{rad} \cdot \mathrm{s}^{2}), \, \mathcal{M} = 4.38 \,\mathrm{kg}, \, l = 0.248 \,\mathrm{m}.$$
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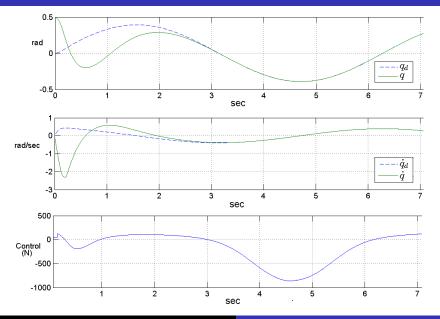
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We took $\tau = 0.07$ s and $A \equiv 1$ and the same model parameters

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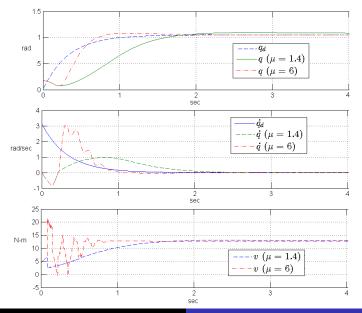
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We used these mismatched parameters in the control:

$$J' = 1.25J, \quad b'_1 = 1.2b_1, \quad b'_2 = 0.9b_2, \quad \bar{a}' = 1.185\bar{a}, \\ b'_3 = 0.85b_3, \quad k'_1 = 1.1k_1, \quad k'_2 = 0.912k_2, \quad \bar{b}' = 0.98\bar{b}, \quad (17) \\ k'_3 = 0.9k_3, \quad \mathcal{M}' = 0.97\mathcal{M}, \quad \text{and} \quad l' = 1.013l.$$



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Tracking Control for Neuromuscular Electrical Stimulation

Summary of NMES Research

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In future work, we hope to apply input-to-state stability to better understand the effects of uncertainties under state constraints.